



UNIVERSITÀ DEGLI STUDI DI GENOVA

Dottorato di ricerca in Biotecnologie in Medicina

Traslazionale

Coordinatore prof. Rodolfo Quarto

Tutor prof. Gianmario Sambuceti

Tesi di Dottorato

**“Effect of starvation on brain glucose
metabolism and 18F-2-fluoro-2-
deoxyglucose uptake:
an experimental in vivo and ex-vivo study.”**

Relatore:

Prof. Gianmario Sambuceti

Candidata:

Dott.ssa Ambra Buschiazzo

Anno Accademico 2017/2018

Index

1. Introduction

2. Materials and methods

- *Animal Models*
- *Experimental micro-PET scanning protocol*
- *Image processing*
- *Ex-vivo experiments*
- *Ex vivo imaging*
- *Brain homogenate analysis*
- *Value K_m and V_{max} for HK*

3. Results

- *MicroPET analysis of in vivo brain response to starvation*
- *Ex vivo evaluation of CMR_{Glu} and CMR_{Glu}^**
- *Starvation effect on determinants of glucose and FDG entrapment*

4. Discussion

5. Conclusions

6. References

Introduction

Under physiological conditions, adult brain exclusively depends on glucose oxidation to fuel the high-energy demand for uptake recycling of neurotransmitters and maintenance of ion gradients [1-3]. Local glucose consumption is thus selectively modulated by neuronal activation while being relatively independent of hormonal whole body-derived signals. These principles represent the physiological basis underlying the clinical value of ^{18}F -fluoro-2-deoxy-glucose (FDG) imaging in different neurodegenerative disorders [4].

Nevertheless, although 'brain metabolic independence' has been consistently documented under physiological conditions, a wide literature also reported a measurable response of brain metabolism to severe starvation [5, 6]. This condition can be frequently encountered in patients with Alzheimer's disease in whom the cognitive impairment can often result in prolonged reduction in food intake with consequent body weight loss.

From the clinical point of view, this impairment contributes to disease progression, particularly in advanced age, as indicated by large epidemiologic studies [7-9]. From the methodological point of view, the possible consequences on diagnostic accuracy of FDG imaging are less certain. In fact, the reduction in glucose availability, combined with the increase in circulating levels of beta-hydroxybutyrate (BHB) and acetoacetate induced by starvation, can switch brain metabolism from a preferential (if not exclusive) glycolytic pattern to a prevalent oxidation of ketone bodies [1,2,10,11]. The consequent reduction in CMRGlu might obviously decrease FDG retention thus asking for dedicated procedures to optimize image quality and counting statistics. On the other hand, the metabolic shift might modify neuronal gene expression profile, promoting the appearance of GLUT carriers and hexokinase isoforms with different affinities for glucose and FDG. This condition might alter the ratio between glucose consumption (CMRGlu) and its index provided by FDG uptake (CMRGlu*) thus modifying the lumped constant value [12,13]. Finally, the systemic adaptation to food deprivation

decreases glucose disposal and FDG sequestration in the whole body, protracting tracer persistence in the bloodstream as to preserve or even increase brain FDG uptake indexed by SUV. The present study aimed to define whether and how the interplay among these three factors induced by starvation interferes with brain FDG uptake and thus with the diagnostic accuracy of PET/CT imaging in neuro-degenerative diseases.

Materials and methods

Animal Models

Six-weeks-old BALB/c female mice (The Charles River Laboratories, Italy) were housed in sterile enclosures under specific pathogen-free conditions. The 30 mice were divided into two groups: 15 animals, “control” group were kept under standard conditions and exposed to fasting for 6 hours before the study; the remaining animals were submitted to 48 hours of starvation (“STS”, absence of food and free access to water) before imaging. In each group, 9 mice were submitted to micro-PET imaging while six mice were sacrificed for the *ex vivo* studies and thus for measurement of FDG uptake (n=3) or biochemical analyses (n=3), respectively.

Experimental micro-PET scanning protocol

In vivo imaging was performed according to our validated procedure [14]. Anaesthesia was induced by intraperitoneal administration of ketamine (100 mg/kg) and xylazine (10 mg/kg). Capillary glucose level and body weight were measured, and mice were positioned on the bed of a dedicated micro-PET system (Albira, Bruker Inc, US). A dose of 3-4 MBq of FDG was then injected through a tail vein, soon after start of a list mode acquisition lasting 50 minutes.

Image processing

List data were divided according to the following framing rate: 10x15 secs, 5x30 secs, 2x150 secs, 6x300 secs, 1x600 secs), and then reconstructed using a maximal likelihood

expectation maximization method (MLEM). Two nuclear doctors unaware of mouse allocation drew a volume of interest (VOI) in the left ventricular chamber to plot the time-concentration curve in arterial blood throughout the whole acquisition (input function). Whole body FDG clearance (in $\text{ml} \times \text{min}^{-1}$) was calculated using the conventional stochastic approach as the ratio between injected dose and integral of input function, fitting the last 20 minutes with a mono-exponential function [15]. In vivo CMRGlu* was estimated according to Gjedde-Patlak [16] graphical analysis by using the routine of dedicated software (PMOD, Zurich, Switzerland) with lumped constant value set at 1. On these parametric maps, two VOIs were drawn to estimate average brain (CMRGlu*) and skeletal muscle (SM-MRGlu*) in $\text{nanoMol} \times \text{min}^{-1} \times \text{g}^{-1}$. These same VOIs were thus transferred on the last 600 secs frame to estimate FDG standardized uptake value (SUV). According to the same procedure, at regional analysis, cortical and cerebellar CMRGlu* and SUV were estimated to calculate the cortical/cerebellum ratio in the two studied subgroups of animals.

Ex-vivo experiments

For 'ex vivo' evaluation, each brain was harvested soon after sacrifice, stuck in the outer ring of a Petri dish with octyl-cyanoacrylate (Dermabond, Ethicon, US) and covered with 2 mL solution collected from an input vial containing 3 mL of DMEM medium (12.5 mM glucose) with a known FDG concentration (1 MBq/mL). Time-activity curve (TAC) of tracer uptake was thus plotted using the Ligand Tracer White device (Ridgeview, Uppsala, Se) [17, 18]. Briefly, this instrument consists of a beta-emission detector and a rotating platform harbouring a standard Petri dish. The rotation axis is inclined at 30° from the vertical, so that the medium covers the dish nadir while the detector points at its zenith. All experiments consisted of 45 periodic rotations lasting one minute and divided into 4 intervals: *a*) brain kept for 25 seconds in the system nadir and thus fully immersed in the incubation medium; *b*) 5 seconds 180° counter-clockwise rotation; *c*) brain kept for 25 seconds under the detector at the system zenith and, finally, *d*) 5 seconds 180° counter-clockwise rotation for cycle restart. At each cycle, the detector measures background and target counting rates (in counts per second,

CPS) in phase *a* and *c*, respectively. FDG brain TAC was thus obtained by subtracting background counting rate from the corresponding target value [19].

At the end of the experiment, an aliquot of 0.5 mL was sampled both from input vial and from Petri dish (output) to measure glucose concentration (mM) and total FDG activity (MBq). Brain TAC was thus normalized by multiplying brain counting rate at each time *t* (BCR(*t*)) for the following factor:

$$BFD(t) = BCR(t) \times \frac{1}{BCR_{(45 \text{ min})}} \times \frac{(A_{input} - A_{output})}{A_{input}} \quad [1]$$

where BFD(*t*) represents the fraction of the dose present in the brain at each time *t*, BCR_(45 min) represents the brain counting rate in the last minute, *A_{input}* and *A_{output}* represent FDG activity in MBq at experiment start and end, respectively.

The closed system nature of Ligand tracer permitted us to consider the input function (IF) as:

$$IF(t) = 1 - BFD(t) \quad [2]$$

BFD(*t*) and IF(*t*) were thus used according to Patlak graphical analysis, assuming the volume invariance of both incubation medium and brain, during the experiment, respectively. The regression line was defined as:

$$\frac{BFD_t}{IF_t} = a \frac{\int_0^t IF_t dt}{IF_t} + b \quad [3]$$

This curve was analysed in order to verify the expected accumulation kinetics of FDG, the slope *a* was identified by least squares definition of regression line and multiplied for input glucose level to estimate CMR_{Glu}*, with the star denoting the FDG-based measurement of CMR_{Glu}, according to the original definition of Sokoloff al [20]. By contrast, ex vivo CMR_{Glu} (in nanoMol × min⁻¹) was measured by the equation:

$$CMR_{Glu} = (\text{Glucose}_{input} - \text{Glucose}_{output}) \left(\frac{\text{nanoMol}}{\text{mL}} \right) \times \frac{2}{45} \left(\frac{\text{ml}}{\text{min}} \right) \quad [4]$$

where glucose represents glucose contraction (nM), 2 is the volume of used DMEM and 45 is the experiment duration.

Ex vivo imaging

Soon after the end of the ex-vivo experiment, brains were washed and frozen in isopentane chilled with dry ice for sectioning with a cryomicrotome in slices 100 μM thick. At least three sections per brain were placed on a microscope slide and exposed to an imaging plate (Cyclone, PerkinElmer, US) that provides an image resolution of 100 μm . Exposure time was optimized to 5 minutes. Thereafter, brain sections were stained with haematoxylin/eosin and photographed by inverted optical microscope. No measurement of radioactivity content was attempted, while autoradiography images were co-registered with the histologic staining using ImageJ software.

Brain homogenate analysis.

For biochemical analyses, brains were homogenized in phosphate-buffer saline (PBS) solution with a Potter-Elvehjem homogenizer. Proteins concentration was performed by Bradford analysis [21]. The samples were sonicated for 10 s in ice.

Western blot experiments were performed accordingly to the standard procedure using 50 μg proteins for each sample. Enzymatic assays were performed spectrophotometrically in a double beam spectrophotometer (UNICAM UV2, Analytical S.n.c., Italy) using 100 μg of protein for each sample.

Activities of hexokinase (HK), phosphofructokinase (PFK), glucose-6-phosphate dehydrogenase (G6PD), G6Pase and Complex I (NADH-ubiquinone oxidoreductase) were assayed according to methods our previously validated procedure [14]. β -Hydroxy-butyrate-dehydrogenase (BHBDH) activity was evaluated following reduction of NAD^+ at 340 nm using a solution of: 200 mM Tris-HCl pH 8, 2 mM NAD^+ , 30 mM β -hydroxybutyrate. Glutathione Reductase activity was evaluated spectrophotometrically, at 405 nm, using Glutathione Reductase Assay Kit (Abcam: ab83461) following the manufacture's instructions. Real-Time PCR evaluation was performed according to the standard procedures of our lab [22].

Value Km and Vmax for HK

Hexokinases (HK) Michaelis-Menten kinetics was evaluated for in the presence of glucose and 2-deoxy-glucose (2DG; Sigma-Aldrich, Saint Louis, MO, US). The kinetic characterization of HK, was determined, at pH 7.4 and 25°C, by coupling hexose phosphorylation to the reduction of NADP, recording the change in absorbance at 340 nm. Studied initial concentrations were 0.05 mM, 0.1 mM, 1 mM, 5 mM and 200 mM for glucose and 0.3 mM, 5 mM, 50 mM, 100 mM and 200 mM for 2DG. To avoid the substrate selectivity, G6PD was substituted with hexose-6P-dehydrogenase (H6PD), as an enzyme able to process both hexoses. V_{max} (the maximum rate achieved by the system) and K_m (the Michaelis-Menten constant indicating the substrate concentration at which the reaction rate is $V_{max}/2$) were determined by Lineweaver-Burk double reciprocal plots.

Statistical analysis

Data are presented as mean \pm standard deviation (SD). For comparison between different groups, the Null hypothesis was tested by Student t test for paired or unpaired data, as appropriate. Significance was considered for p values $p < 0.05$. Statistical analyses were performed using SPSS software 15.0 (Chicago, Illinois).

Results

MicroPET analysis of in vivo brain response to starvation

STS caused a significant reduction in body weight (12.7 ± 0.3 vs 16.9 ± 0.9 grams, in starved mice and controls, respectively, $p < 0.001$) while its effect on serum glucose level was less pronounced (3.78 ± 1.65 vs 4.78 ± 1.62 mmol/L, respectively, $p = 0.15$). Blood clearance of FDG was significantly lower in starved mice with respect to control ones (0.03 ± 0.01 vs 0.05 ± 0.01 mL \times min⁻¹, $p < 0.01$).

Compartmental analysis of dynamic micro-PET scans documented a significant response of brain metabolism to STS. In fact, both average slope of Patlak regression line (0.013 ± 0.007 vs 0.027 ± 0.010 min⁻¹, respectively, $p < 0.001$) and CMRGlu*

(46.1 ± 23.3 vs 119.5 ± 40.2 nanomol \times min⁻¹ \times g⁻¹, respectively, $p < 0.001$) were lower in starved than in control mice (Figure #1). By contrast, the STS-related drop in whole body glucose disposal, and the consequent prolongation of tracer availability in the bloodstream, preserved FDG uptake in the brain, whose average SUV was even (though not significantly) higher in STS than in control mice (2.59 ± 0.36 vs 2.00 ± 0.66 , respectively, $p = 0.14$, Figure #1). At regional analysis, CMRGlucose* and SUV cortical/cerebellum ratio remained remarkably stable in both STS and control mice.

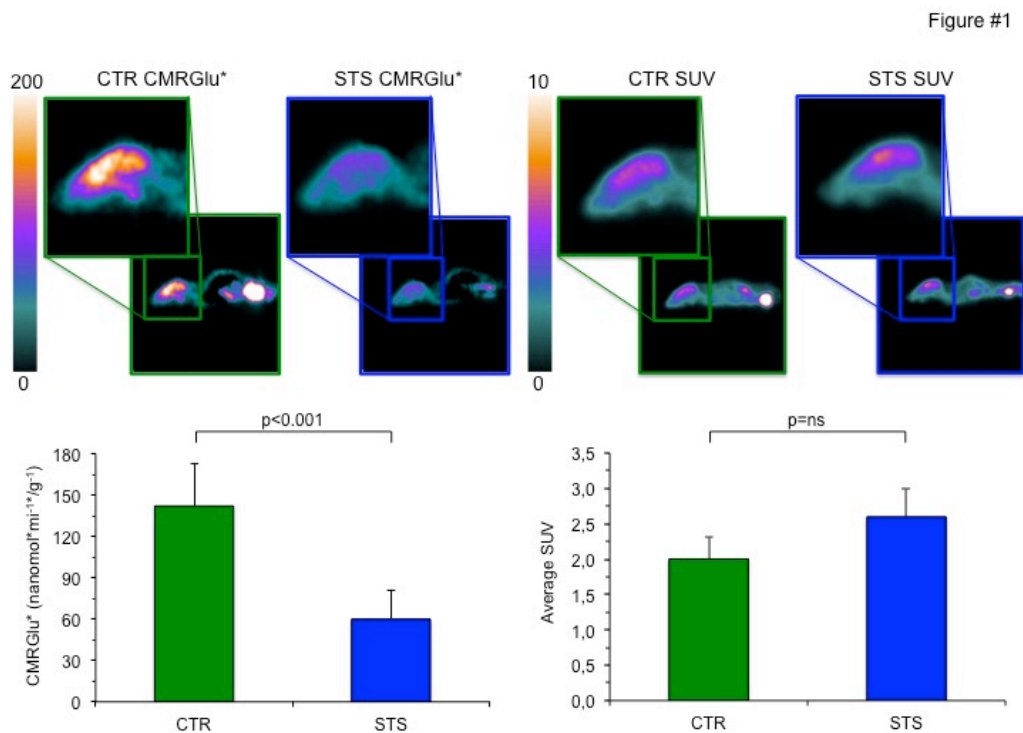


Figure 1. In vivo effect of STS on brain metabolism. In the upper part, on the left, brain parametric maps of representative control (CTR) and 48 hours starved (STS) mice are shown; representative images of basal metabolic activity of the whole brain expressed in average standardized uptake value (SUV) are shown on the right. In the bottom, graphs of whole cerebral metabolic rate of glucose (CMRGlucose*; nanomol \times min⁻¹ \times g⁻¹) and SUV are displayed, respectively. Results indicate mean \pm SD of 9 mice per group; green bars represent control value, blue bars represent STS value.

This metabolic response was largely different in skeletal muscles (SM) as confirmed by the marked decrease in both hind limbs SM-MRGlucose* (0.2 ± 0.15 vs 1.02 ± 0.4 nanomol \times g⁻¹ \times min⁻¹ respectively, $p < 0.01$) and average SUV (0.22 ± 0.1 vs 0.54 ± 0.3 , respectively, $p < 0.01$) in starved mice with respect to controls (Figure #2).

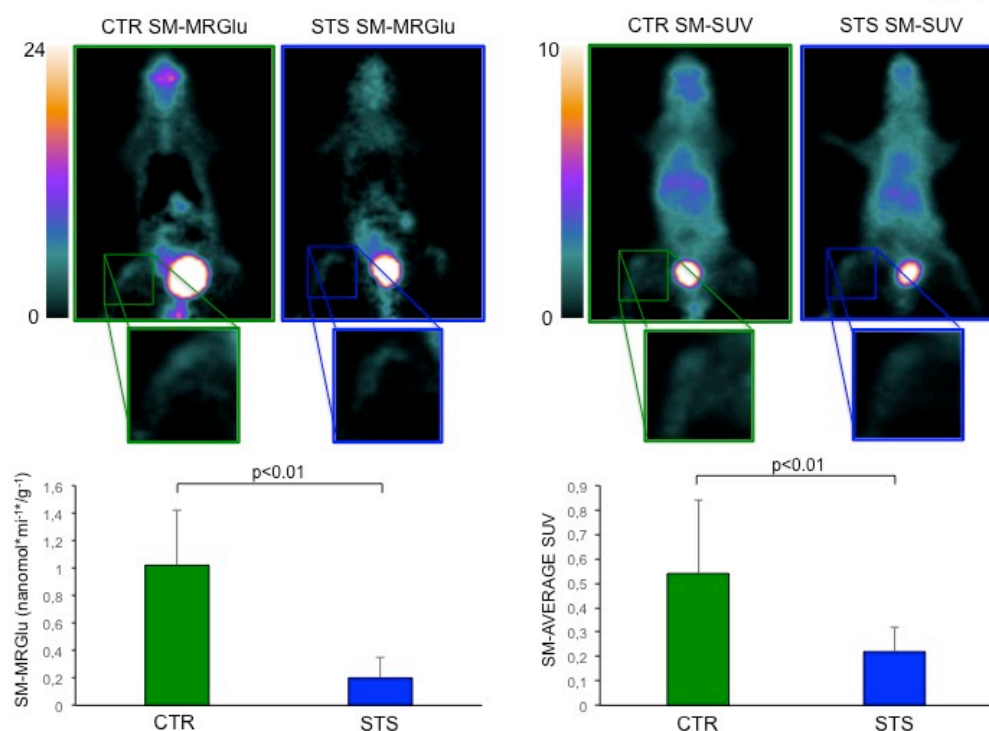


Figure 2. In vivo effect of STS on skeletal muscle metabolism. In the upper part, on the left, skeletal muscle parametric maps of representative control (CTR) and 48 hours starved (STS) mice are shown; representative images of basal metabolic activity of hind limbs skeletal muscle expressed in average standardized uptake value (SUV) are shown on the right. In the bottom, graphs of hind limbs skeletal muscle metabolic rate of glucose (SM-MRGlu*; nanomol * min⁻¹ * g⁻¹) and SUV are displayed, respectively. Results indicate mean±SD of 9 mice per group; green bars represent control value, blue bars represent STS value.

*Ex vivo evaluation of CMRGlu and CMRGlu**

Autoradiography and its co-registration with haematoxylin/eosin staining documented the expected selectivity of tracer uptake in the grey matter, confirming the viability of all six studied brains during the 45 minutes incubation (Figure #3, Panel A).

The *ex vivo* evaluation confirmed the STS effect on brain metabolism documented in vivo. Despite identical extracellular environments, previous 48 hours food deprivation markedly reduced all indexes of brain hexose intake. In fact, fractional drop of glucose concentration in the incubation medium was markedly lower in starved than in control mice (0.05 ± 0.02 vs 0.11 ± 0.04 %, respectively, $p < 0.05$, Figure #3, Panel B). A similar observation also applied to the fractional loss of FDG (Figure #3, Panel C) from the incubation medium that was almost halved in brains explanted from starved mice (0.037 ± 0.015 %) with respect to control ones (0.075 ± 0.02 %; $p < 0.01$).

Obviously, this same response was documented by the estimation of metabolic rates. In fact, CMRGlu was 61.1 ± 16.1 nanomol \times min⁻¹ in control preparations and decreased to 28.27 ± 12.7 nanomol \times min⁻¹ in STS ones ($p < 0.01$). This response closely agreed with the corresponding CMRGlu*. In all brains, FDG time-activity curves showed a linear increase during the whole experiment (Figure #3, Panel D) and thus confirmed the expected accumulation kinetics of FDG. Similarly, Patlak regression plot showed a good correlation with r values always ≥ 0.97 . Again, previous STS decreased CRMGl* from 38.3 ± 11 to 17.8 ± 7.2 nanomol \times min⁻¹ ($p < 0.05$, Figure #3, Panel D).

As a consequence, lumped constant value was not affected by nutritional status. In fact, the ratio between fractional removals of FDG and glucose from the medium was superimposable in control and STS brains as well as the ratio CMRGlu* / CMRGlu (Figure #3, Panel E).

Figure #3

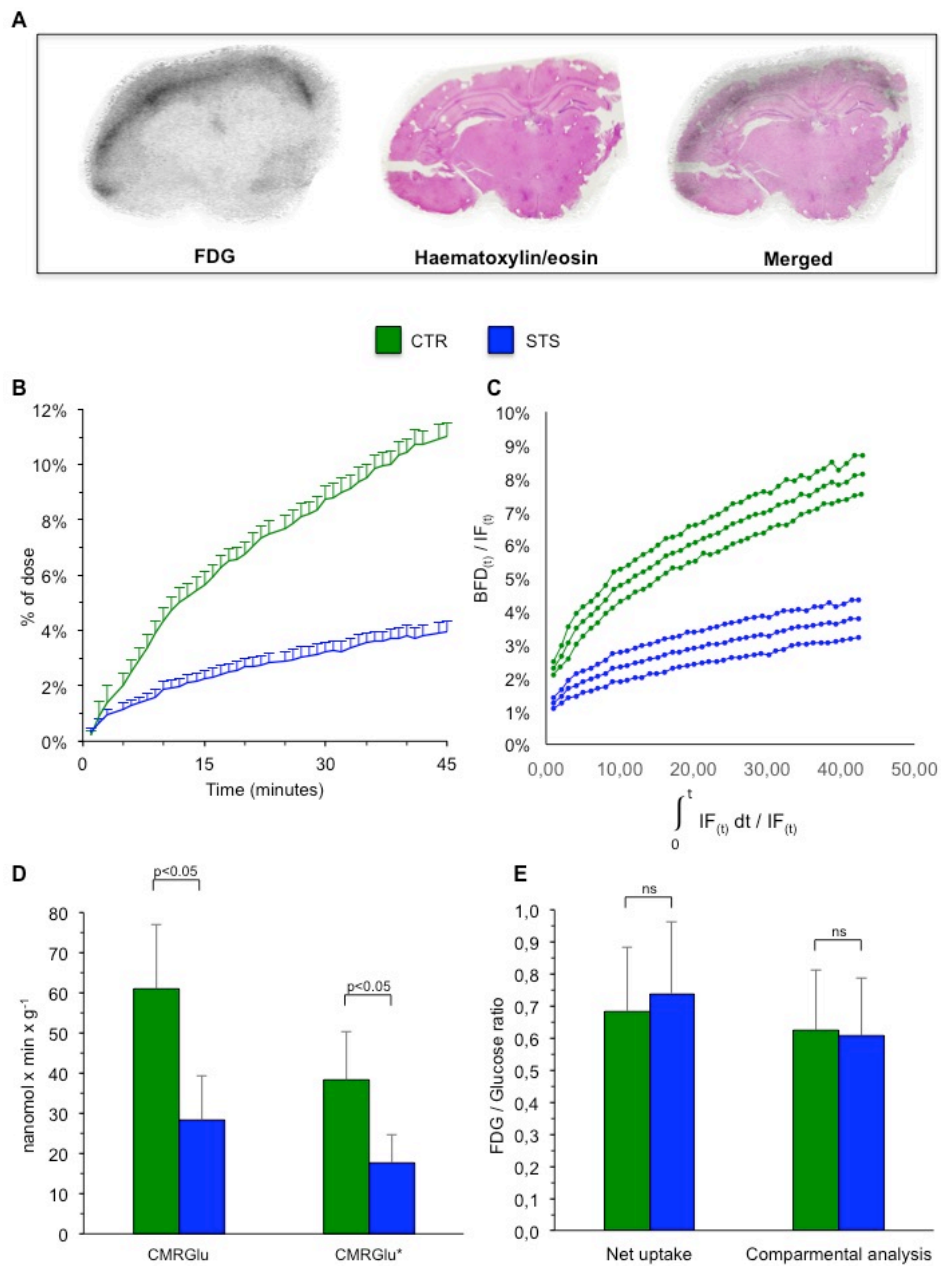


Figure 3. Ex vivo evaluation of CMRGlu and CMRGlu*. Panel A reports the autoradiography (first image), its co-registration with haematoxylin/eosin staining (second picture) and the merge of the two results (third image). Panel B reports the FDG time-activity curves expressed in % of dose, Panel C reports the Patlak regression plot. In each graph, control (CTR) mice are represented in green and starved (STS) mice in blue. Panel D reports the CMRGlu (left) and CMRGlu* (right) values expressed in nanomol \times min \times g $^{-1}$, Panel E reports the lumped constant value obtained as CMRGlu* / CMRGlu.

Starvation effect on determinants of glucose and FDG entrapment

The marked reduction in glucose consumption and FDG uptake induced by STS was not explained by changes in the membrane hexose carriers. In fact, protein levels (Figure #4, Panel A) of the different GLUTs (GLUT 1-2-3-4) were remarkably stable regardless nutritional status.

A similar response was documented for HK isoforms. Coherently with the literature [23], HKs gene expression profiling of brain homogenates documented high levels of mRNA encoding for HK isoform I, with only trace signals for isoforms HKII, HKIII and HKIV. Nutritional status did not significantly affect neither HKs expression profile (Figure #4, Panel B) nor kinetic features of hexose phosphorylation. In fact, estimated V_{\max} (Figure #4 Panel C) and K_m (Figure #4, Panel D) of HK-related catalysis were only trivially affected by STS for both glucose and 2DG confirming the theoretical basis for the observed lumped constant invariance.

Although the expression of G6Pase was very low in controls, Western blot analysis demonstrated a slight and not significant reduction of protein amount in starved brains (Figure #4, Panel E). On the other hand, the activity of G6Pase were found to be extremely low in brain homogenates under normal conditions and remained unchanged regardless nutritional status (Figure #4, Panel F).

Figure #4

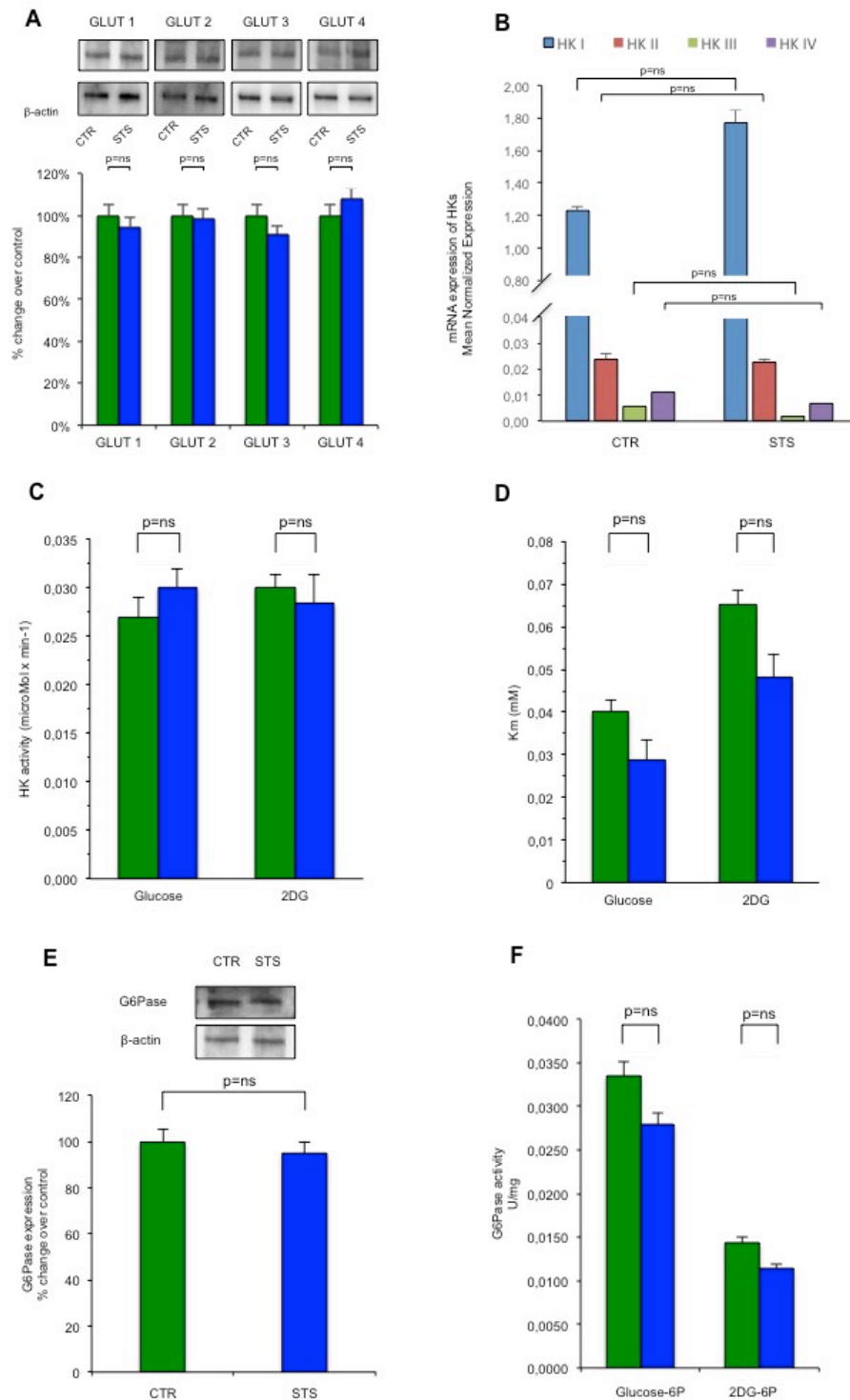


Figure #4: STS effect on determinants of glucose and FDG entrapment. Panel A reports the western blot analysis against GLUT1, GLUT2, GLUT3 and GLUT4 performed in brain homogenate of control (CTR, green bars) and of starved mice (STS, blue bars). Protein levels of the different GLUTs isoform were remarkably stable regardless nutritional status. Data were expressed in % change over control \pm SD of at least three experiments. The values have been normalized on β -actin. Panel B reports the HK gene expression profiling of brain homogenates in CTR (left) and STS mice (right), obtained by Real-time PCR. The four different isoforms have been analyzed: HK I (blue bar), HK II (red bar), HK III (green bar) and HK IV (purple bar). Results are expressed in Mean Normalized Expression \pm SD. Nutritional status did not affect this expression profile. Panel C reports the HK activity of brain homogenate in CTR mice (green bar) and in STS mice (blue bar) in presence of glucose (left) and 2DG (right). Data are expressed in micromol \times min⁻¹ \pm SD of at least three experiments. Panel D reports HK Km expressed determined by Lineweaver-Burk double reciprocal plots. Data are expressed in mM \pm SD of at least three experiments. Panels E and F report the

western blot analysis against G6Pase and the G6Pase activity, respectively. In both graphs, CTR group is represented in green and the STS mice in blue. Western blot results are expressed in % change over control \pm SD of at least three experiments. Values have been normalized on β -actin. The G6Pase activity was assayed in presence of glucose-6P (left) and 2DG-6P (right) and the values are expressed in U x mg of proteins-1 \pm SD of at least three experiments.

On the contrary, STS significantly reduced the catalytic activity of PFK, the rate-limiting enzyme of glycolysis, ($3.7 \pm 0.6 \times 10^{-2}$ vs $5.6 \pm 0.1 \times 10^{-2}$ mU/mg of proteins in STS and control brains respectively, $p < 0.01$, Figure #5, Panel A). In agreement with this response, lactate release slightly decreased (though not significantly) from 28 ± 9 in controls to 19 ± 6 nanomol \times min⁻¹ in STS-mice ($p = 0.20$). The evident reduction in glycolytic flux was not counterbalanced by any response of PPP since its regulator G6PD showed constant mRNA levels (0.35 ± 0.01 vs 0.30 ± 0.02 mean normalized expression in control and STS brains, respectively, $p = ns$), protein abundance (Figure #5, Panel B) and activity (Figure #5, Panel C).

As expected, the reduced hexose avidity induced by STS was paralleled by a metabolic shift from a prevalent glycolytic pattern to a preferential oxidation of ketone bodies [24]. This concept was confirmed by the evaluation of BHBDH activity that markedly increased in STS brain lysates with respect to control ones (6.41 ± 0.96 vs 0.64 ± 0.09 mU/mg of proteins, respectively, $p < 0.01$, Figure #5, Panel D). Similarly, it was corroborated by the response of respiratory Complex I, whose activity significantly increased in STS-brain with respect to controls (0.92 ± 0.06 vs 0.59 ± 0.04 U/mg of proteins, respectively, $p < 0.01$; Figure #5, Panel E). Finally, and in line with the respiratory burst intrinsically associated with ketone bodies catabolism, glutathione reductase, showed a significant increase after STS (Figure #5 Panel F).

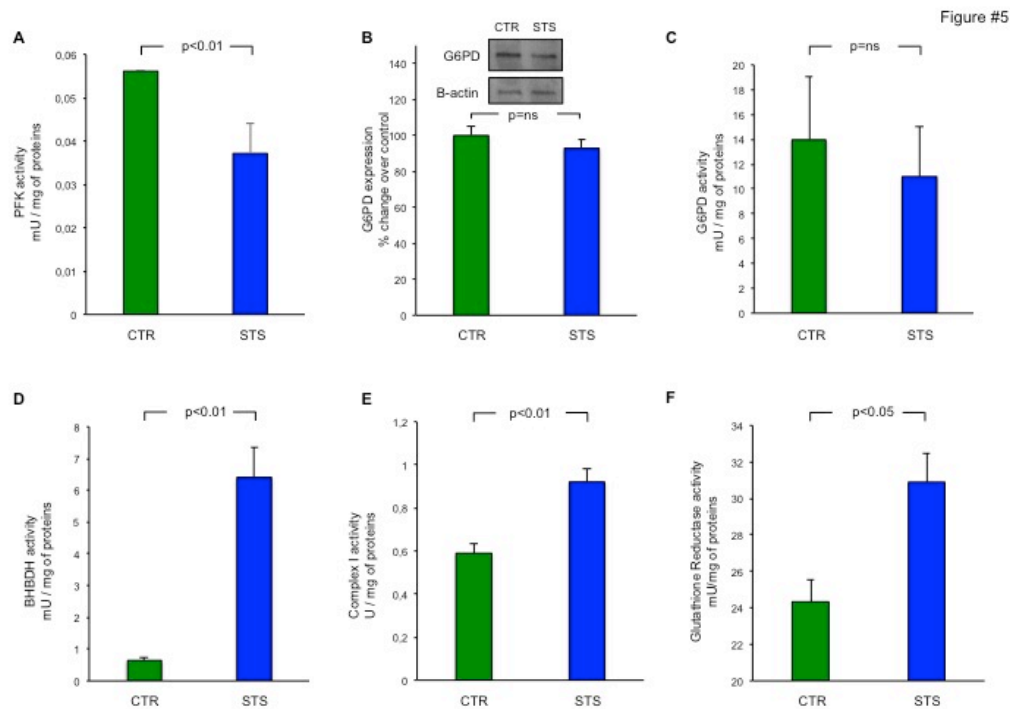


Figure #5: Metabolic machinery of starved brain. In each panel of Figure #5, green bars represent the brain homogenate of control (CTR) mice and the blue bars represent the brain homogenate of starved (STS) mice. Panel A reports the PFK activity expressed in mU x mg of proteins-1± SD of at least three experiments. The catalytic activity was reduced in STS-brain homogenate with respect to CTR. Panels B and C report western blot analysis and enzyme activity of G6PD, respectively. Western blot results are expressed in % change over control ± SD of at least three experiments. Values have been normalized on β-actin. Values of G6PD activity are expressed in U x mg of proteins-1± SD of at least three experiments. Panels D, E and F report enzyme activities of BHBDH (expressed in mU x mg of proteins-1), Complex I (U x mg of proteins-1) and Glutathione reductase (mU x mg of proteins-1), respectively, ± SD of at least three experiments.

Discussion

The present study documents that starvation markedly decreases brain glucose consumption without altering measured FDG SUV in mouse experimental models. This apparent paradox does not reflect any change in lumped constant since the ratio between tracer uptake and glucose intake remains remarkably constant regardless nutritional condition. Rather, it is explained by the metabolic response of the whole body: the decrease in FDG sequestration by the skeletal muscle is as profound as to prolong tracer persistence in the bloodstream and thus its availability for brain uptake.

Biochemical Considerations

In the present study, control CMRGlu* was comparable to the data reported by Kreissl et al in mice exposed to a similar fasting duration [25]. However, this value was almost halved after 48 hours STS. In agreement with the evident decrease in PFK [26] activity,

this response confirms previous studies showing a profound deceleration in brain glycolytic rate after prolonged food deprivation and weight loss both in humans [5,6] and rodents [27]. A similar consideration applies to the almost fivefold increase of BHBDH activity in starved brains. This observation agrees with the acknowledged brain metabolic response to STS in which the preferential utilization of ketone bodies [28] accelerates cell respiration as confirmed by the enhancement in mitochondrial Complex I function. Similarly, the relatively low OXPHOS efficiency [24] of ketolysis, and the consequent rise in reactive oxygen species, nicely explains the increase in glutathione-reductase activity [29] as a basic cell response to oxidative stress.

Accordingly, the observed halving of CMRGlu* induced by STS is coherent with a marked reduction in brain glycolytic flux compensated by an accelerated ketolysis. Although blood levels of ketone bodies were not tested in our models, this concept is largely confirmed by the ex vivo part of our study. Explanted STS brains were immersed in a medium with high glucose concentrations and without any other competing substrate. Under this condition, the reduced avidity for glucose and FDG persisted in all brains harvested from STS mice suggesting a profound shift in the metabolic machinery of studied nervous tissues.

Methodological considerations.

Besides its biochemical relevance, the pilot ex vivo evaluation provides a direct experimental and theoretical evidence of lumped constant stability under severe food deprivation. Previous attempts to approach this issue in vivo obtained conflicting results: the compartmental analysis applied by Redies and coworkers [6] reported an STS-related reduction in lumped constant that was not confirmed by Hasselbalch et al [30] who compared CMRGlu (measured by Fick method) with CMRGlu* (measured by brain kinetics of FDG uptake).

Our ex vivo approach permitted us to couple tracer-based estimation of CMRGlu* with the direct measurement of CMRGlu. The ratio between these two variables remained remarkably stable in brains harvested from normally fed or starved mice. The stability of lumped constant was confirmed by the invariance of its theoretical determinants.

According to the original Sokoloff statement, the ratio between glucose intake and 2DG uptake reflects the different affinities for the two hexoses of factors regulating transmembrane transport, hexose phosphorylation and de-phosphorylation: GLUT expression (λ) was not affected by STS and, similarly, G6Pase activity (ϕ) on both glucose and 2DG was unchanged regardless nutritional condition. Moreover, direct measurements of K_m and V_{max} for both glucose and 2DG documented an absent effect of STS on HK isoforms affinity for the two hexoses.

Accordingly, 'ex vivo' experiments indicate that the observed response of CMR_{Glu}^* to STS did reflect a profound reduction in brain glycolytic rate. The preserved (or even slightly increased) brain FDG SUV observed in starved mice was instead explained by the relatively more profound impairment in glucose utilization by the whole body of starved mice. This response has been already reported in the literature as a possible consequence of the increased blood concentration of ketone bodies under starvation [31]. In agreement with this study, the severe (almost fivefold) reduction in skeletal muscle avidity for FDG profoundly altered tracer kinetics virtually halving its blood clearance (Figure #6, Panel A). The decreased CMR_{Glu} halved the tracer extraction fraction in STS brain (Figure #6, Panel B). As a consequence, FDG brain retention increased more slowly in starved mice with respect to control ones. However, the longer duration of tracer availability prolongs the uptake process up to values higher with respect to control SUVs (Figure #6, Panel C).

Altogether the present study indicates that STS actually impairs brain glycolytic flux as documented by the similar decrease in both CMR_{Glu} and CMR_{Glu}^* . This response reflects an adaptation in the enzymatic machinery of cells populating the central nervous system and persists under exposure to high glucose concentration without the competition of any other metabolite.

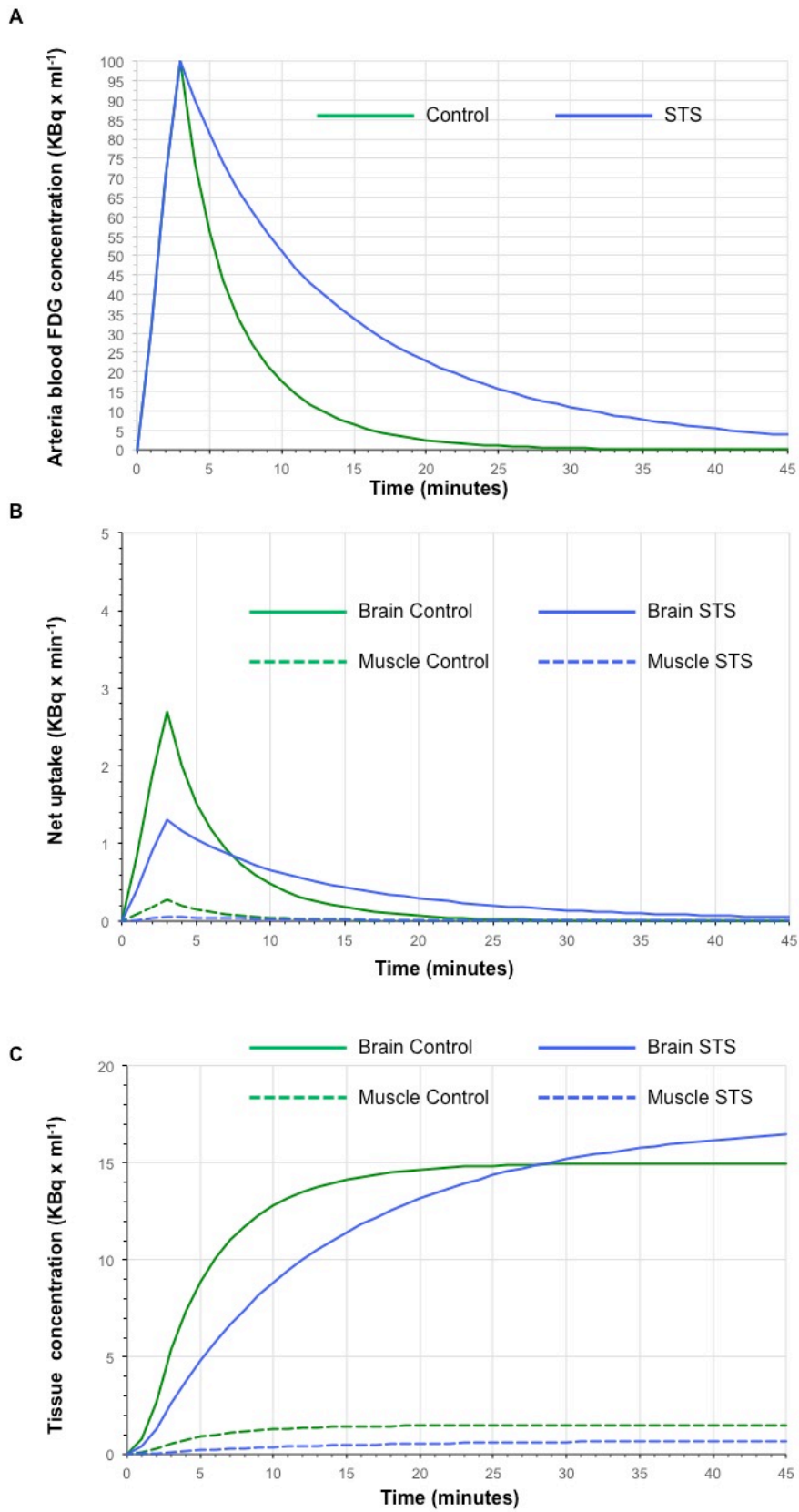


Figure #6: Theoretical model of FDG uptake in brain and skeletal muscle. This cartoon represents a theoretical model for FDG uptake in brain and skeletal muscles in control (green) and STS (blue) mice. Panel A displays FDG arterial concentration as predicted by the corresponding average clearance value measured in the two groups: the decreased tracer sequestration by the whole body prolongs tracer availability in the bloodstream. Panel B represents the

instantaneous uptake ($\text{KBq} \times \text{min}^{-1}$). The curves are defined assuming an identical flow rate in the two conditions, with final uptake values only justified by the interaction between extraction fraction and tracer availability. Brain and skeletal muscle are represented by solid and dotted lines, respectively. Panel C displays time-concentration curves in the two tissues and points out the progressive increase in STS brain as a consequence of the prolonged tracer availability. Despite a virtual halving of extraction fraction the prolonged uptake phase eventually results in preserved FDG uptake at later times. This phenomenon is markedly less evident in the skeletal muscle due to the relatively more severe (fivefold vs twofold) reduction in glucose consumption.

Conclusions

From the methodological point of view, the present findings confirm the theoretical limitations of brain SUV as a surrogate of CMRGlucose^* in estimating brain glucose consumption. However, the clinical interpretation of FDG imaging mostly relies on the identification of relative metabolic inhomogeneities as markers of neurodegenerative disorders. The virtually absent response of FDG SUV to STS thus further confirms the adequacy of current procedures even in underfed patients provided that time gap between injection and imaging is carefully respected. Defining the regional distribution of STS effect throughout the different cortical areas was not possible with our experimental model. The relevance of this limitation is indicated by documented heterogeneity in metabolic response to food deprivation in the different brain structures [32, 33]. Nevertheless, the severe brain metabolic impairment induced by STS indicates a possible predictive power of regional CMRGlucose^* . This potential might configure dynamic PET studies to evaluate the link between nutritional status and neurodegeneration.

References

1. Clarke DD, Sokoloff L. Circulation and energy metabolism of the brain. In: Siegel G, Agranoff B, Albers RW and Fisher S (eds) Basic neurochemistry: Molecular, cellular, and medical aspects. 6th ed. Philadelphia: Lippincott-Raven, 1999. pp. 637-669.
2. Dienel GA. Energy metabolism in the brain. In: Byrne JH and Roberts JL (eds) From molecules to networks: An introduction to cellular and molecular neuroscience. 2nd ed. London: Academic Press, 2009. pp. 49-110.
3. Attwell D, Laughlin SB. An energy budget for signaling in the grey matter of the brain. *J Cereb Blood Flow Metab.* 2001;21:1133-45.
4. Garibotto V, Herholz K, Boccardi M, Picco A, Varrone A, Nordberg A, Nobili F, Ratib O; Geneva Task Force for the Roadmap of Alzheimer's Biomarkers. Clinical validity of brain fluorodeoxyglucose positron emission tomography as a biomarker for Alzheimer's disease in the context of a structured 5-phase development framework. *Neurobiol Aging.* 2017;52:183-95.
5. Owen OE, Morgan AP, Kemp HG, Sullivan JM, Herrera MG, Cahill GF. Brain metabolism during fasting. *J Clin Invest.* 1967;46:1589-95.
6. Redies C, Hoffer LJ, Beil C, Marliss EB, Evans AC, Lariviere F, Marrett S, Meyer E, Diksic M, Gjedde A, et al. Generalized decrease in brain glucose metabolism during fasting in humans studied by PET. *Am J Physiol.* 1989;256:E805-10.
7. Emmerzaal TL, Kiliaan AJ, Gustafson DR. 2003-2013: a decade of body mass index, Alzheimer's disease, and dementia. *J Alzheimers Dis.* 2015;43:739-55.
8. Gao S, Nguyen JT, Hendrie HC, Unverzagt FW, Hake A, Smith-Gamble V, Hall K. Accelerated weight loss and incident dementia in an elderly African-American cohort. *J Am Geriatr Soc.* 2011;59:18-25.
9. Johnson DK, Wilkins CH, Morris JC. Accelerated weight loss may precede diagnosis in Alzheimer disease. *Arch Neurol.* 2006;63:1312-7.
10. Hawkins RA, Biebuyck JF. Ketone bodies are selectively used by individual brain regions. *Science.* 1979;205:325-27.

11. Hasselbalch SG, Madsen PL, Hageman LP, Olsen KS, Justesen N, Holm S, Paulson OB. Changes in cerebral blood flow and carbohydrate metabolism during acute hyperketonemia. *Am J Physiol.* 1996;270:E746-51.
12. Bøtker HE, Goodwin GW, Holden JE, Doenst T, Gjedde A, Taegtmeier H. Myocardial glucose uptake measured with fluorodeoxyglucose: a proposed method to account for variable lumped constants. *J Nucl Med.* 1999;40:1186-96.
13. Graham MM, Muzi M, Spence AM, O'Sullivan F, Lewellen TK, Link JM, Krohn KA. The FDG lumped constant in normal human brain. *J Nucl Med.* 2002;43:1157-66.
14. Marini C, Bianchi G, Buschiazzo A, Ravera S, Martella R, Bottoni G, Petretto A, Emionite L, Monteverde E, Capitanio S, Inglese E, Fabbi M, Bongioanni F, Garaboldi L, Bruzzi P, Orengo AM, Raffaghello L, Sambuceti G. Divergent targets of glycolysis and oxidative phosphorylation result in additive effects of metformin and starvation in colon and breast cancer. *Sci Rep.* 2016;6:19569.
15. Marini C, Salani B, Massollo M, Amaro A, Esposito AI, Orengo AM, Capitanio S, Emionite L, Riondato M, Bottoni G, Massara C, Boccardo S, Fabbi M, Campi C, Ravera S, Angelini G, Morbelli S, Cilli M, Cordera R, Truini M, Maggi D, Pfeffer U, Sambuceti G. Direct inhibition of hexokinase activity by metformin at least partially impairs glucose metabolism and tumor growth in experimental breast cancer. *Cell Cycle.* 2013;12:3490-9.
16. Patlak CS, Blasberg RG, Fenstermacher JD. Graphical evaluation of blood-to-brain transfer constants from multiple-time uptake data. *J Cereb Blood Flow Metab.* 1983;3:1-7.
17. Björke H, Andersson K. Automated, high-resolution cellular retention and uptake studies in vitro. *Appl Radiat Isot.* 2006;64:901-5.
18. Björke H, Andersson K. Measuring the affinity of a radioligand with its receptor using a rotating cell dish with in situ reference area. *Appl Radiat Isot.* 2006;64:32-7.
19. Mertens K, Mees G, Lambert B, Van de Wiele C, Goethals I. In vitro 2-deoxy-2-[18F]fluoro-D-glucose uptake: practical considerations. *Cancer Biother Radiopharm.* 2012;27:183-8.
20. Sokoloff L, Reivich M, Kennedy C, Des Rosiers MH, Patlak CS, Pettigrew KD, Sakurada O, Shinohara M. The [14C]deoxyglucose method for the measurement of

local cerebral glucose utilization: theory, procedure, and normal values in the conscious and anesthetized albino rat. *J Neurochem.* 1977;28:897-916.

21. Bradford MM. A rapid and sensitive method for the quantitation of microgram quantities of protein utilizing the principle of protein-dye binding. *Anal Biochem.* 1976;72:248-54.

22. Balza E, Castellani P, Moreno PS, Piccioli P, Medraño-Fernandez I, Semino C, Rubartelli A. Restoring microenvironmental redox and pH homeostasis inhibits neoplastic cell growth and migration: therapeutic efficacy of esomeprazole plus sulfasalazine on 3-MCA-induced sarcoma. *Oncotarget.* 2017;8: 67482-96.

23. Muzi M, Freeman SD, Burrows RC, Wiseman RW, Link JM, Krohn KA, Graham MM, Spence AM. Kinetic characterization of hexokinase isoenzymes from glioma cells: implications for FDG imaging of human brain tumors. *Nucl Med Biol.* 2001;28:107-16.

24. Prince A, Zhang Y, Croniger C and Puchowicz M. Oxidative metabolism: glucose versus ketones. *Adv Exp Med Biol.* 2013;789:323-8.

25. Kreissl MC, Stout DB, Wong KP, Wu HM, Caglayan E, Ladno W, Zhang X, Prior JO, Reiners C, Huang SC, Schelbert HR. Influence of dietary state and insulin on myocardial, skeletal muscle and brain [¹⁸F]-fluorodeoxyglucose kinetics in mice. *EJNMMI Res.* 2011;1:8.

26. Ruderman NB, Ross PS, Berger M, Goodman MN. Regulation of glucose and ketone-body metabolism in brain of anaesthetized rats. *Biochem J.* 1974;138:1-10.

27. Corddry DH, Rapoport SI, London ED. No effect of hyperketonemia on local cerebral glucose utilization in conscious rats. *J Neurochem.* 1982;38:1637-41.

28. Cahill GF. Starvation in man. *N Engl J Med.* 1970;282:668–75.

29. Korge P, Calmettes G, Weiss JN. Increased reactive oxygen species production during reductive stress: The roles of mitochondrial glutathione and thioredoxin reductases. *Biochim Biophys Acta – Bioenerg.* 2015;1847:514-25.

30. Hasselbalch SG, Knudsen GM, Jakobsen J, Hageman LP, Holm S, Paulson OB. Brain metabolism during short-term starvation in humans. *J Cereb Blood Flow Metab.* 1994;14:125-31.

31. Wu GY, Thompson JR. The effect of ketone bodies on alanine and glutamine metabolism in isolated skeletal muscle from the fasted chick. *Biochem J.* 1988;255:139-44.
32. Yanagisawa M, Planel E, Ishiguro K, Fujita SC. Starvation induces tau hyperphosphorylation in mouse brain: implications for Alzheimer's disease. *FEBS Letter.* 1999;461:329-33.
33. Jimenez A, Pegueroles J, Carmona-Iragui M, Vilaplana E, Montal V, Alcolea D, Videla L, Illán-Gala I, Pané A, Casajoana A, Belbin O, Clarimón J, Moizé V, Vidal J, Lleó A, Fortea J, Blesa R; Alzheimer's Disease Neuroimaging Initiative. Weight loss in the healthy elderly might be a non-cognitive sign of preclinical Alzheimer's disease. *Oncotarget.* 2017;8:104706-16.